

Introduction to the Finite Element Method

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Outline

1. First definitions
2. Presentation of the Laplacian problem
3. Theoretical results: existence and uniqueness of the solution
4. Discretization : Finite element method
5. Numerical resolution and convergence of the method
6. Example of application

First definitions / reminder 😊

Formulation of the problem

Finite element method

Numerical resolution

Application: ophthalmology

Functional spaces

Let $\Omega \subset \mathbb{R}^d$ be a bounded domain with boundary $\partial\Omega$. We define the following functional spaces:

- ▶ $L^2(\Omega) = \{u : \Omega \rightarrow \mathbb{R} \mid \int_{\Omega} |u|^2 dx < +\infty\}$, the space of square-integrable functions on Ω .
- ▶ $H^1(\Omega) = \left\{ u \in L^2(\Omega) \mid \frac{\partial u}{\partial x_i} \in L^2(\Omega) \text{ for all } i = 1, \dots, d \right\}$, the Sobolev space of functions with square-integrable first derivatives.
- ▶ $H_0^1(\Omega) = \{u \in H^1(\Omega) \mid u = 0 \text{ on } \partial\Omega\}$, the subspace of $H^1(\Omega)$ whose functions vanish on the boundary.

They have infinite dimension.

We also define the norms associated with these spaces:

- ▶ L^2 norm: $\|u\|_{L^2(\Omega)} = \sqrt{\int_{\Omega} |u|^2 dx}$
- ▶ H^1 norm: $\|u\|_{H^1(\Omega)} = \sqrt{\|u\|_{L^2(\Omega)}^2 + \sum_{i=1}^d \left\| \frac{\partial u}{\partial x_i} \right\|_{L^2(\Omega)}^2}$

Tiny remark on derivative

- ▶ In the definition of $H^1(\Omega)$, the derivatives $\frac{\partial u}{\partial x_i}$ are understood in the **weak sense** (distributional derivative).
- ▶ A function $u \in L^2(\Omega)$ has a weak derivative $\frac{\partial u}{\partial x_i} \in L^2(\Omega)$ if there exists a function $v \in L^2(\Omega)$ such that for all test functions $\varphi \in C_c^\infty(\Omega)$ (smooth functions with compact support):

$$\int_{\Omega} u \frac{\partial \varphi}{\partial x_i} dx = - \int_{\Omega} v \varphi dx$$

In this case, we write $v = \frac{\partial u}{\partial x_i}$.

Hilbert spaces

Definition

A *Hilbert space* is a complete inner product space, i.e., a vector space $\mathcal{H}$ equipped with an inner product $\langle \cdot, \cdot \rangle_{\mathcal{H}}$ such that every Cauchy sequence in $\mathcal{H}$ converges to an element in $\mathcal{H}$.

Theorem

The spaces $L^2(\Omega)$, $H^1(\Omega)$, and $H_0^1(\Omega)$ are Hilbert spaces with the inner products defined as follows:

► L^2 inner product: $\langle u, v \rangle_{L^2(\Omega)} = \int_{\Omega} uv dx$

► H^1 inner product: $\langle u, v \rangle_{H^1(\Omega)} = \langle u, v \rangle_{L^2(\Omega)} + \sum_{i=1}^d \left\langle \frac{\partial u}{\partial x_i}, \frac{\partial v}{\partial x_i} \right\rangle_{L^2(\Omega)}$

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Position of the problem

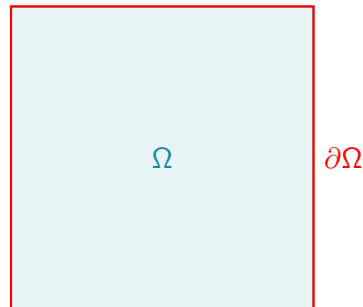
- ▶ We have a bounded domain $\Omega \subset \mathbb{R}^d$ with boundary $\partial\Omega$.
- ▶ We consider the problem of **heat transfer** in Ω given by the **partial differential equation** (PDE):

$$\begin{cases} -\Delta u = f & \text{in } \Omega, \\ u = 0 & \text{on } \partial\Omega. \end{cases}$$

With $f \in L^2(\Omega)$ is a given source term, and u is the unknown temperature field.

- ▶ Δ is the **Laplace operator**, defined as the divergence of the gradient:

$$\Delta u = \frac{\partial^2 u}{\partial x^2} + \frac{\partial^2 u}{\partial y^2}$$



Variational formulation

- We multiply the PDE by a test function $v \in H_0^1(\Omega)$ and integrate over Ω :

$$\int_{\Omega} (\Delta u) v dx = - \int_{\Omega} f v dx$$

- Using integration by parts (Green's identity), we have:

$$- \int_{\Omega} \nabla u \cdot \nabla v dx + \int_{\partial\Omega} (\nabla u \cdot n) v d\sigma = - \int_{\Omega} f v dx$$

- Since $v = 0$ on $\partial\Omega$, the boundary term vanishes, leading to the variational formulation: Find $u \in H_0^1(\Omega)$ such that

$$a(u, v) = \ell(v) \quad \forall v \in H_0^1(\Omega)$$

where

$$a(u, v) = \int_{\Omega} \nabla u \cdot \nabla v dx, \quad \ell(v) = \int_{\Omega} f v dx$$

Existence of a solution

Theorem: Lax–Milgram

Let V be a Hilbert space. Let $a: V \times V \rightarrow \mathbb{R}$ be a bilinear form that is :

- ▶ **Continuous:** There exists a constant $C > 0$ such that $|a(u, v)| \leq C\|u\|_V\|v\|_V$ for all $u, v \in V$.
- ▶ **Coercive:** There exists a constant $\alpha > 0$ such that $a(u, u) \geq \alpha\|u\|_V^2$ for all $u \in V$.

Let $\ell: V \rightarrow \mathbb{R}$ be a continuous linear functional ($\exists C > 0$ such that $|\ell(v)| \leq C\|v\|_V$ for all $v \in V$).

Then there exists a unique $u \in V$ such that

$$a(u, v) = \ell(v) \quad \forall v \in V$$

Checking the hypotheses of Lax–Milgram

For our problem:

$$a(u, v) = \int_{\Omega} \nabla u \cdot \nabla v dx, \quad \ell(v) = \int_{\Omega} f v dx$$

- **Continuity of a and ℓ :** follows from Cauchy–Schwarz — an integral of a product is controlled by the product of L^2 norms. No surprise here.

Checking the hypotheses of Lax–Milgram

For our problem:

$$a(u, v) = \int_{\Omega} \nabla u \cdot \nabla v dx, \quad \ell(v) = \int_{\Omega} f v dx$$

- ▶ **Coercivity of a** is the one real question: does $a(u, u) = \|\nabla u\|_{L^2}^2$ control the *full* norm $\|u\|_{H^1}^2 = \|u\|_{L^2}^2 + \|\nabla u\|_{L^2}^2$?
- ▶ At first glance: no — a only sees the gradient, not u itself.
- ▶ **This is exactly where $u = 0$ on $\partial\Omega$ saves us:** the **Poincaré inequality** says that on $H_0^1(\Omega)$, a function is controlled by its own gradient:

$$\exists C_{\Omega} > 0, \quad \|u\|_{L^2(\Omega)} \leq C_{\Omega} \|\nabla u\|_{L^2(\Omega)} \quad \forall u \in H_0^1(\Omega)$$

- ▶ Intuitively: if u vanishes on the boundary, it can't be large anywhere without its gradient being large too.

So for our problem, there exists a unique solution $u \in H_0^1(\Omega)$ such that

$$a(u, v) = \ell(v) \quad \forall v \in H_0^1(\Omega)$$

First definitions / reminder 😊

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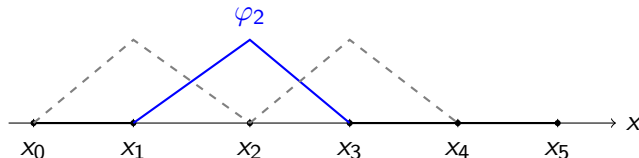
Application: ophthalmology

Finite element discretization (in 1D)

We define a finite dimensional subspace $V_N \subset V = H_0^1(\Omega)$.

- ▶ Discretize $\Omega = [0, L]$ with nodes $0 = x_0 < x_1 < \dots < x_N < x_{N+1} = L$
- ▶ Define $V_N = \{v \in C^0(\overline{\Omega}) : v|_{[x_i, x_{i+1}]} \text{ affine, } v(0) = v(L) = 0\}$
- ▶ **Notation:** $\mathbb{P}_1(\Omega)$ is the space of piecewise affine functions on Ω
- ▶ Basis: the **hat functions** $(\varphi_i)_{i=1, \dots, N}$, one per interior node, satisfying

$$\varphi_i(x_j) = \delta_{ij} = \begin{cases} 1 & \text{if } i = j \\ 0 & \text{else} \end{cases}$$



Finite element discretization (in 1D)

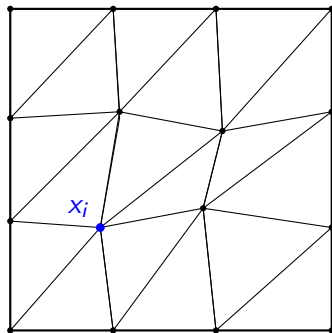
- ▶ $(\varphi_i)_{i=1,\dots,N}$ is a **basis** of V_N : it is free and spanning by construction, so $\dim V_N = N$
- ▶ **Nodal interpolation**: since $\varphi_i(x_j) = \delta_{ij}$, any $v_N \in V_N$ writes uniquely as

$$v_N = \sum_{i=1}^N v_N(x_i) \varphi_i$$

i.e. the coefficients are simply the values of v_N at the nodes

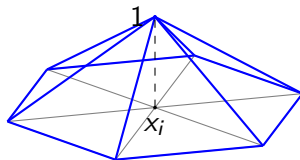
Finite element space in 2D

Discretize Ω by a **triangulation** $\mathcal{T}_h$ with nodes $(x_i)_{i=1,\dots,N}$:



- ▶ $V_N = \{v \in C^0(\overline{\Omega}) : v|_T \text{ affine on each triangle } T, v = 0 \text{ on } \partial\Omega\}$
- ▶ $\dim(V_N) = N$ (one basis function per interior node)

Shape of a 2D basis function φ_i



- ▶ φ_i is the **pyramid (tent) function**: value 1 at x_i , affine on each surrounding triangle, 0 on the boundary of the patch and beyond
- ▶ Same properties as in 1D: $\varphi_i(x_j) = \delta_{ij} \dots$

First definitions / reminder 😊

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Algorithm to solve the variational problem

1. Discretize the domain Ω into a mesh of elements (triangles in 2D, tetrahedra in 3D).
2. Choose a finite element space V_h and construct the basis functions $\{\varphi_i\}$.
3. Assemble the stiffness matrix $\underline{\underline{\mathbf{A}}} \in \mathbb{R}^{N \times N}$ and load vector $\underline{\mathbf{b}} \in \mathbb{R}^N$:

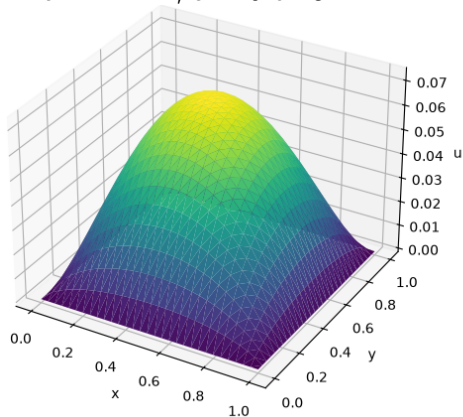
$$\underline{\underline{\mathbf{A}}}_{ij} = a(\varphi_j, \varphi_i) = \int_{\Omega} \nabla \varphi_j \cdot \nabla \varphi_i dx,$$

$$\underline{\mathbf{b}}_i = \ell(\varphi_i) = \int_{\Omega} f \varphi_i dx.$$

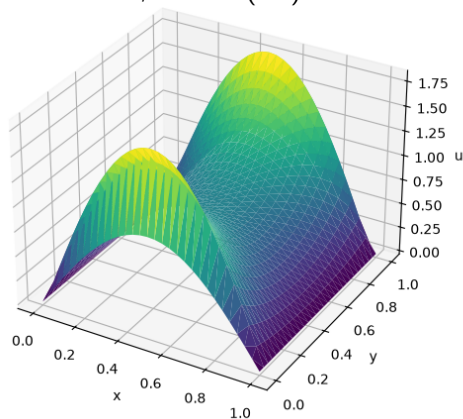
4. Solve the linear system $\underline{\underline{\mathbf{A}}}\mathbf{u} = \underline{\mathbf{b}}$ for the coefficients $\mathbf{u} = (u_1, u_2, \dots, u_N) \in \mathbb{R}^N$.

First results

$$-\Delta u = 1 \text{ in } \Omega, u = 0 \text{ on } \partial\Omega$$



$$-\Delta u = 0 \text{ in } \Omega, u = \sin(\pi x) \text{ on } \partial\Omega$$



Convergence of the method

Convergence of the finite element method

The theoretical convergence rate for piecewise linear elements is $\mathcal{O}(h)$ in the H^1 norm and $\mathcal{O}(h^2)$ in the L^2 norm, where h is the maximum element diameter.

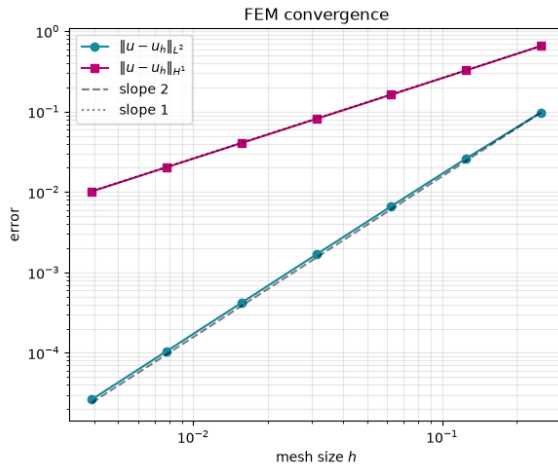
- ▶ The function $u_{\text{exact}}(x, y) := \sin(\pi x) \sin(\pi y)$ is the exact solution to the problem:

$$\begin{cases} -\Delta u = 2\pi^2 \sin(\pi x) \sin(\pi y) & \text{in } \Omega, \\ u = 0 & \text{on } \partial\Omega. \end{cases}$$

- ▶ We compute the numerical solution u_h using the finite element method on a sequence of refined meshes.
- ▶ As we picked u_{exact} , we can measure the error directly.



Convergence of the method



First definitions / reminder 😊

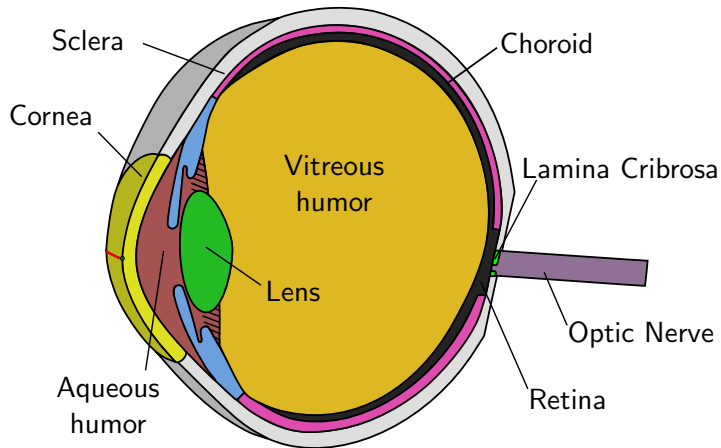
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Geometry of the eye



$$\Omega = \bigcup_i \Omega_i$$

Biophysical model

- ▶ We study the **flow** of the aqueous humor in the anterior chamber of the eye, coupled with the **heat transfer** in the eye.
- ▶ The steady flow of the aqueous humor is governed by the Navier–Stokes equations:

Navier-Stokes equations

Boussinesq approximation

$$\rho(\vec{u} \cdot \nabla) \vec{u} - \nabla \cdot (2\mu \mathbf{D}(\vec{u}) - p\mathbf{I}) = -\rho\beta(T - T_{\text{ref}})\vec{g} \quad \text{in } \Omega_{\text{AH}},$$

Incompressibility

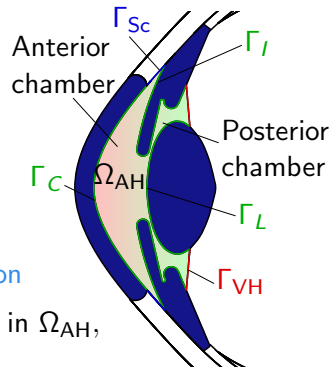
$$\nabla \cdot \vec{u} = 0$$

in $\Omega_{\text{AH}},$

Heat transfer equation

$$\rho C_p \vec{u} \cdot \nabla T - k_i \Delta T = 0$$

in $\Omega = \bigcup_i \Omega_i.$



Three unknown quantities: (i) the **fluid velocity** $\vec{u}$, (ii) its **pressure** p , and (iii) the **temperature** of the eye T .

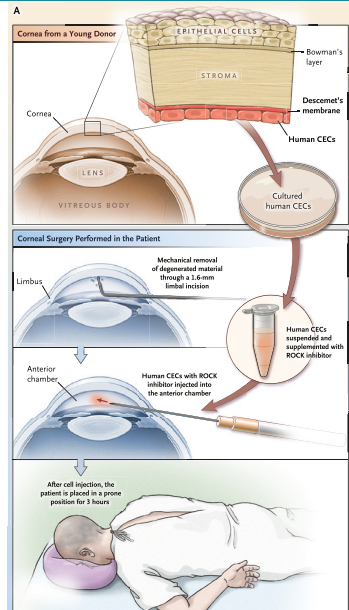
Motivation: Endothelial cells sedimentation

- ▶ AH flow plays a significant role in heat distribution, and intraocular pressure^a.

💡 Medical application: **corneal endothelial cell sedimentation** in the cornea^b.

^aDvoriashyna *et al.* *Ocular Fluid Dynamics*. (2019)

^bKinoshita *et al.* *N Engl J Med*. (2018) (Figure extracted from this reference)



Weak formulation

We define the following functional spaces :

1. The *velocity* space $\mathbf{V} := [H_0^1(\Omega_{\text{AH}})]^3$, consisting of vector fields $\vec{u}$ with square-integrable derivatives with a trace that vanishes on the boundary;
2. the *pressure* space $Q := L_0^2(\Omega_{\text{AH}}) = \left\{ p \in L^2(\Omega_{\text{AH}}) \middle| \int_{\Omega_{\text{AH}}} p \, dx = 0 \right\}$, consisting of square-integrable scalar fields with zero mean; and
3. the *temperature* space $W := H^1(\Omega)$.

Weak formulation

Find $(\vec{u}, p, T) \in \mathbf{V} \times Q \times W$ such that for all $(\vec{v}, q, \varphi) \in \mathbf{V} \times Q \times W$:

$$\begin{aligned} \rho \int_{\Omega_{\text{AH}}} (\vec{u} \cdot \nabla) \vec{u} \cdot \vec{v} dx + \mu \int_{\Omega_{\text{AH}}} \mathbf{D}(\vec{u}) : \nabla \vec{v} dx - \int_{\Omega_{\text{AH}}} p \cdot \nabla \vec{v} dx \\ + \int_{\Omega_{\text{AH}}} \rho_0 \beta T \vec{g} \cdot \vec{v} dx = \int_{\Omega_{\text{AH}}} \rho_0 \beta T_{\text{ref}} \vec{g} \cdot \vec{v} dx, \end{aligned}$$

$$\int_{\Omega_{\text{AH}}} \nabla \cdot \vec{u} q dx = 0,$$

$$\begin{aligned} \rho C_p \int_{\Omega} \vec{u} \cdot \nabla T \varphi dx + k \int_{\Omega} \nabla T \cdot \nabla \varphi dx + \int_{\Gamma_{\text{amb}}} (h_{\text{amb}} T d\sigma + \sigma \varepsilon T^4) \varphi d\sigma + \int_{\Gamma_{\text{body}}} h_{\text{bl}} T \varphi d\sigma \\ = \int_{\Gamma_{\text{amb}}} (h_{\text{amb}} T_{\text{amb}} + \sigma \varepsilon T_{\text{amb}}^4) \varphi d\sigma + \int_{\Gamma_{\text{body}}} h_{\text{bl}} T_{\text{bl}} \varphi d\sigma. \end{aligned}$$

Weak formulation

Find $(\vec{u}, p, T) \in \mathbf{V} \times Q \times W$ such that for all $(\vec{v}, q, \varphi) \in \mathbf{V} \times Q \times W$:

$$\begin{aligned} a_1(\vec{u}, \vec{u}, \vec{v}) + a_2(\vec{u}, \vec{v}) + b(p, \vec{v}) + d(T, \vec{v}) &= \ell_1(\vec{v}), \\ b(q, \vec{u}) &= 0, \\ e(\vec{u}, T, \varphi) + f(T, \varphi) &= \ell_2(\varphi). \end{aligned}$$

Weak formulation

Find $(\vec{u}, p, T) \in \mathbf{V} \times Q \times W$ such that for all $(\vec{v}, q, \varphi) \in \mathbf{V} \times Q \times W$:

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- ▶ $\mathbf{V}_h := \left\{ \vec{v} \in [\mathbb{P}_2(\Omega_{\text{AH}})]^3 \mid \vec{v} = \vec{0} \text{ on } \partial\Omega \right\}$, the space of vector-valued piecewise quadratic polynomials that vanish on the boundary for velocity;
- ▶ $Q_h := \mathbb{P}_1(\Omega_{\text{AH}})$, the space of piecewise linear polynomials for pressure; and
- ▶ $W_h := \mathbb{P}_1(\Omega)$, the space of piecewise linear polynomials for temperature.

Weak formulation

The algebraic problem to solve is then :

$$\begin{bmatrix} \underline{\underline{\mathbf{V}^k}} + \underline{\underline{\mathbf{W}^k}} + \underline{\underline{\mathbf{N}}} & \underline{\underline{\mathbf{B}^T}} & \underline{\underline{\mathbf{D}}} \\ & \underline{\underline{\mathbf{B}}} & \underline{\underline{\mathbf{0}}} \\ & \underline{\underline{\mathbf{E}_1^k}} & \underline{\underline{\mathbf{E}_2^k}} + \underline{\underline{\mathbf{F}}} \end{bmatrix} \begin{bmatrix} \underline{\underline{\Delta u}} \\ \underline{\underline{\Delta p}} \\ \underline{\underline{\Delta T}} \end{bmatrix} = \begin{bmatrix} \underline{\underline{\mathbf{r}_{\vec{u}}^k}} \\ \underline{\underline{\mathbf{r}_p^k}} \\ \underline{\underline{\mathbf{r}_T^k}} \end{bmatrix},$$

Problem of dimension $\dim(\mathbf{V}_h) + \dim(Q_h) + \dim(W_h)$.

In this example :

- ▶ $\dim(\mathbf{V}_h) = 2.42 \cdot 10^5$
- ▶ $\dim(Q_h) = 7.08 \cdot 10^5$
- ▶ $\dim(W_h) = 34,304$

Pressure and velocity: impact of the posture

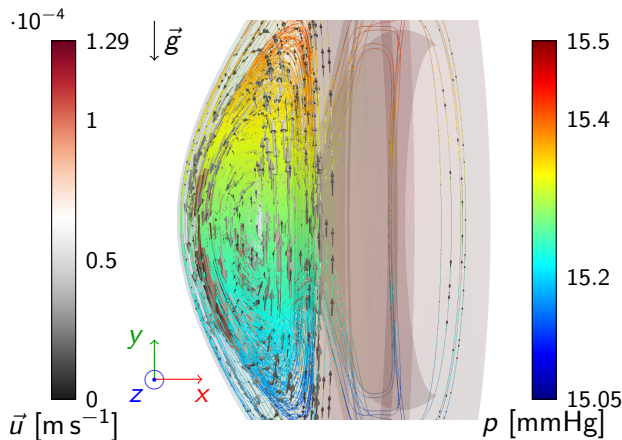


Figure: Standing position.

► **Recirculation of the AH,**

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- ^aWang *et al.* BioMedical Engineering OnLine. (2016)
^bAbdelhafid *et al.* Recent Devel. in Mathematical, Statistical and Computational Sciences. (2021)
^cMurgoitio-Esandi *et al.* Translational Vision Science & Technology. (2023)

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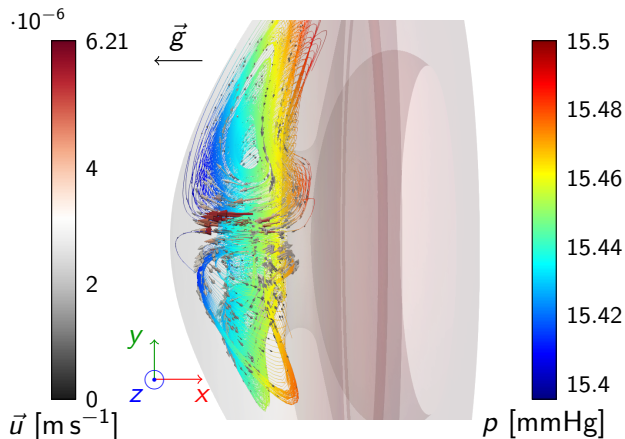


Figure: Prone position.

- **Recirculation** of the AH,
- Formation of a **Krukenberg's spindle**, in good agreement with clinical observations and previous studies^{abc}

^aWang *et al.* BioMedical Engineering OnLine. (2016)

^bAbdelhafid *et al.* Recent Dev. in Mathematical, Statistical and Computational Sciences. (2021)

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Pressure and velocity: impact of the posture

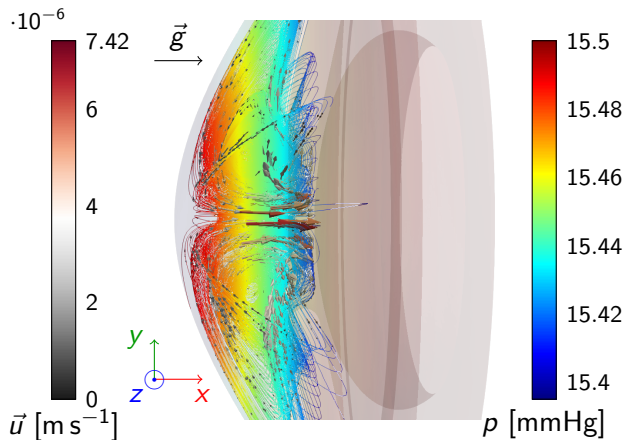


Figure: Supine position.

- ▶ **Recirculation** of the AH,
- ▶ Formation of a **Krukenberg's spindle**, in good agreement with clinical observations and previous studies^{abc}
- ▶ Fluid dynamics is **strongly influenced by the position of the patient**.

^aWang *et al.* BioMedical Engineering OnLine. (2016)

^bAbdelhafid *et al.* Recent Dev. in Mathematical, Statistical and Computational Sciences. (2021)

^cMurgoitio-Esandi *et al.* Translational Vision Science & Technology. (2023)

Thank you for your attention!
Any question ?

